Compressed Sensing in Optics: Schlieren Deflectometry and Refractive Index Map Reconstruction

Joint work with:

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Compressed Sensing

Highly compressed recap of what is ...

Part I:

Compressive Sensing

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Generally, sampling is ...



Human readable signal!



Generally, sampling is ...

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New ways to sample signals

"Computer readable" sensing + prior information



Generally, sampling is ...

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New ways to sample signals structures, sparsity, low-rank, ...

"Computer readable" sensing + prior information



Compressed Sensing...

... in a nutshell:

"Forget" Dirac, forget Nyquist, ask *few* (**linear**) *questions* about your informative (**sparse**) signal, and recover it *differently* (**non-linearly**)"





Croup



2nd, CS \ni Non-linear reconstruction!



If \boldsymbol{x} is <u>K-sparse</u> and if $\boldsymbol{\Phi}$ well "conditioned" then: $\boldsymbol{x}^* = \underset{\boldsymbol{u} \in \mathbb{R}^N}{\operatorname{arg min}} \|\boldsymbol{u}\|_1 \text{ s.t. } \boldsymbol{y} = \boldsymbol{\Phi} \boldsymbol{u}$ $\|\boldsymbol{u}\|_1 = \sum_j |u_j|$ (Basis Pursuit) [Chen, Donoho, Saunders, 1998]

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2nd, $CS \ni Non-linear$ reconstruction! Simplifying assumption <u>Restricted Isometry Property</u> $\exists \delta \in (0,1)$ $\sqrt{1-\delta} \, \|oldsymbol{v}\|_2 \ \leqslant \ \|oldsymbol{\Phi}oldsymbol{v}\|_2 \ \leqslant \ \sqrt{1+\delta} \, \|oldsymbol{v}\|_2$ for all 2K sparse signals \boldsymbol{v} . any subset of 2K columns is an *isometry* If x is K-sparse and if Φ well "conditioned" then:

$$egin{aligned} oldsymbol{x}^* &= rgmin_{oldsymbol{u} \in \mathbb{R}^N} & \|oldsymbol{u}\|_1 ext{ s.t. } oldsymbol{y} = oldsymbol{\Phi}oldsymbol{u} \ & ext{ if } \delta < \sqrt{2} - 1 \ \|oldsymbol{e}\| \| \|_1 = \sum_j |u_j| \end{aligned}$$
 (Basis Pursuit) [Chen, Donoho, Saunders, 1998]

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2nd, $CS \ni Non-linear reconstruction!$









<u>Part II:</u> Compressive Schlieren Deflectometry

 $({\rm main\ contributor:\ Prasad\ Sudhakar} \\ + Lambda-X\ collaboration\)$

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The problem:



- Local curvature at every \boldsymbol{p} is characterized by $\boldsymbol{s}_{\boldsymbol{p}}(\theta, \varphi)$
- \blacktriangleright Objective: Reconstruct deflection spectra at all p
- Application: Optical manufacturing and metrology

Deflection spectrum:

• Observation:

Smooth objects = controlled deflections = sparse deflection spectra

- Difficult to measure deflections directly
 Only indirect measurement
- <u>Tool: Schlieren Deflectometry</u>

Light changes its path based on refractive index change



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Schlieren deflectometry:

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Measurements are here! Spatial Light Modulator Object Lens 2 Pinhole Lens 3 CCD Lens 1 (SLM) kUniform \mathcal{T} Backlight **H** OSource Deflection \iff Shift Telecentric system (TS) Allows light rays parallel to O $\Delta x = f \tan \theta_k.$ $y_{ik} = \langle oldsymbol{arphi}_i, oldsymbol{s}_k angle$ Deflection Inner product of SLM pattern Optics Spectrum the spectrum with e.g., Fourier $= y_{ik}$ SLM pattern or Hadamard $oldsymbol{arphi}_i$ \boldsymbol{s}_k Elementwise product

A system view ...



The inverse problem

$$\boldsymbol{y}_k = \boldsymbol{\Phi} \boldsymbol{s}_k + \boldsymbol{n}$$

For each pixel k, Obtain $oldsymbol{s}_k$ from $oldsymbol{y}_k$

- Operational requirement
 - Fewer SLM patterns = small sized \boldsymbol{y}_k underdetermined linear inverse problem
- What helps?

- \blacktriangleright sparse deflection spectra ${\boldsymbol s}_k$
- pattern randomness

Compressive Sensing (CS)

CS of deflection spectra



• Rice University's single pixel camera



Each CCD pixel of Schlieren deflectometer = single pixel camera

Image credits: Rice University http://dsp.rice.edu/cscamera

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What are the sensing constraints ?

- Physical constraints of the system:
 - ▶ Non-negative, real-valued sensing matrix entries
 - Binary sensing matrix entries: avoiding non-linearities
- Additional requirements:

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- Randomness for optimal measurements
- Structured measurements for fast computations

Spread Spectrum Compressive Sensing [Puy et al, 2012]

Spread Spectrum Compressive Sensing 1/2

• $\Gamma = H$: Hadamard basis (binary)

Need not be incoherent with the sparsity basis $\,\Psi\,$

- Spread spectrum: random phase modulation of \boldsymbol{s}
 - Rademacher/ Steinhaus sequence $\boldsymbol{m}, |m_i| = 1$ $M = \begin{bmatrix} \boldsymbol{M} \\ \in \mathbb{C}^{N \times N} \end{bmatrix} \quad \boldsymbol{M} = \boldsymbol{H}_{\Omega}^T \boldsymbol{M} \boldsymbol{S}$ $\Phi = \boldsymbol{H}_{\Omega}^T \boldsymbol{M}$
- Real valued $M \Rightarrow m_i = \pm 1$ w.e.p. $\Rightarrow H^T M \in \{\pm 1\}^{N \times N}$
- ▶ Bias and scale for non-negativity: (since optical)

$$\boldsymbol{\Phi} = \frac{1}{2} (\boldsymbol{H}_{\Omega}^{T} \boldsymbol{M} + \boldsymbol{1}_{N} \boldsymbol{1}_{N}^{T}) \in \{0, 1\}^{M \times N}$$

Spread Spectrum Compressive Sensing 2/2

• Universal sensing bases $|\Gamma_{ij}| = \text{const.}$

e.g., Fourier and Hadamard bases

• Successful recovery when $M \ge C_{\rho} K \log^{5}(N)$ with a probability at least $1 - O(N^{-\rho}), 0 < \rho < \log^{3}(N)$ whatever the sparsity basis!! (principle: *coherence* decreasing with spread spec.)

G. Puy, et al., "Universal and efficient compressed sensing by spread spectrum and application to realisticFourier imaging techniques," Journal on Adv. in Sig. Proc., 2012.

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Reconstructions

 $\underbrace{\text{Synthesis:}}_{\boldsymbol{\alpha} \in \mathbb{C}^N} \quad \widehat{\boldsymbol{\alpha}} := \underset{\boldsymbol{\alpha} \in \mathbb{C}^N}{\operatorname{arg\,min}} \quad \|\boldsymbol{\alpha}\|_1 \text{ subject to } \|\boldsymbol{y} - \boldsymbol{\Phi}_{\mathrm{S}} \boldsymbol{\alpha}\|_2 \leq \epsilon \text{ and } \boldsymbol{\Psi} \boldsymbol{\alpha} \in \mathbb{R}^N_+;$



Reconstructions



Reconstructions



- Ψ :DWT & UDWT (Daubechies 9/7 wavelet basis)
- Additional constraint: Non-negative spectra
- Numerically: Proximal methods (Chambolle-Pock algorithm)
 - Generalized gradient methods for non-smooth convex functions
 - (Not detailed here) **Proximal operators:** easy to evaluate for several functions
 - Easy to include additional constraints

Noise estimation (an important part)

- ▶ No test object: Physical model of deflection spectrum
 - deflection spectra = image of the pinhole.

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a disk with a certain radius r and height h.

 \blacktriangleright Without any object, obtain $\boldsymbol{y}^{\mathrm{no}}$ with 100% measurements

$$\Phi^* y^{\text{no}} s^{\text{no}} s^{\text{no}}$$

$$= \sum_{\substack{\text{Model spectrum} \\ \text{spectrum} \\ \text{with } M = N}} \epsilon(N) = \left\| y^{\text{no}} - \Phi_{M=N} \right\|_{2}$$

$$\left\{ \text{For } M < N, \quad \epsilon(M) = \sqrt{M + 2\sqrt{M}} \epsilon(N) / \sqrt{N} \right\} \simeq 5 \text{ dB!}$$

$$(\text{for all } M)$$





Journée thématique conjointe GDR/ISIS et GDR/SoC-SiP 28

Reconstruction results with experimental data

- ▶ Lambda-X NIMO system (9.99D plano-convex lens)
 - ▶ SLM size of 64×64 (one pixel "k")





 $100\%~(M\!/\!N\!)$

<u>Reminder</u>: input SNR $\simeq 5 \, \text{dB!}$

Reconstruction rea

- Lambe
 - $\blacktriangleright SLM \text{ size of } 64 \times 64 \text{ (one pixel "k")}$



 $100\%~(M\!/\!N\!)$

3.6% Synthesis DWT

3.6% Analysis UDWT (similar to synthesis UDWT)



Reconstruction results with experimental data

 \widehat{s}_k : Compressive sensing reconstruction

 $\widehat{\boldsymbol{s}}_{k}^{N}$: spectrum reconstructed with 100% measurements.



Deflection spectrum and the angles



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Deflection radius r vs CCD pixel



Deflection radius γ vs CCD pixel





Main deflection without reconstruction? 1/2

- $\widehat{\boldsymbol{S}}_k$ characterized by $\widehat{\tau}_k = (\overline{c}_k^x, \overline{c}_k^y)^T$.
- $\boldsymbol{g}_{\tau}^{\rho}:$ 2D Gaussian





Location of dominant deflection.

with radius ρ , translated by τ .

- Matched filtering $\hat{\tau}_k = \underset{\tau}{\arg \max} |\langle \hat{s}_k, g_{\tau}^{\rho} \rangle|.$
- Efficiently implemented as convolution
- Can we do something similar in compressive domain?

Main deflection without reconstruction? 2/2

Compressive matched filtering **Smashed filtering***



* M. A. Davenport et al., "Signal processing with compressive measurements," IEEE J. Sel. T. Sig. Proc., 2010.

Visualization plot

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Plot of each r for CCD pixel:



Multifocal diffractive IOL: 2 Dioptric powers 28D and 30.25D



Visualization plot

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Plot of each r for CCD pixel:



Summary and further work

- A real world instance of compressive sensing in action ... and its use
- Practical systems pose their own challenges
- Further...
 - Detailed noise modeling + calibration + nonlinearities
 - Multiple-location reconstruction
 - Consideration of system's PSF:
 blind compressive deconvolution

<u>Part III:</u> Optical Deflectometry

(main contributor: Adriana Gonzalez)



Optical Deflectometric Tomography Interest Intraocular

- Optical characterization of (transparent) objects ODT
- Tomographic Imaging Modality

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Measures light deviation caused by the difference in the object refractive index





lenses

Optical fibers

Optical Deflectometric Tomography Interest Intraocular

- Optical characterization of (transparent) objects ODT
- Tomographic Imaging Modality

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Measures light deviation caused by the difference in the object refractive index \boldsymbol{e}_2







lenses

How to measure light deflections?

• We use our Schlieren Deflectometer (See Part 2)

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Continuous model

Mathematical Model

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- Eikonal equation $\mathcal{R} \text{ curved} : \mathbf{r}(s) \rightarrow \frac{\mathrm{d}}{\mathrm{d}s} (\mathfrak{n} \frac{\mathrm{d}}{\mathrm{d}s} \mathbf{r}(s)) = \mathbf{\nabla} \mathfrak{n}$
- Approximation small $\alpha \to \mathcal{R}$ straight : $\mathbf{r} \cdot \mathbf{p}_{\theta} = \tau$ error < 10% $\alpha(\tau, \theta) = \sin(\alpha)$

$$\alpha(\tau,\theta) = \frac{1}{\mathfrak{n}_{\mathrm{r}}} \int_{\mathbb{R}^2} \left(\boldsymbol{\nabla} \mathfrak{n}(\mathbf{r}) \cdot \mathbf{p}_{\theta} \right) \, \delta(\tau - \mathbf{r} \cdot \mathbf{p}_{\theta}) \, \mathrm{d}^2 \mathbf{r}$$



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Continuous model

Mathematical Model

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- Eikonal equation $\mathcal{R} \text{ curved} : \mathbf{r}(s) \rightarrow \frac{\mathrm{d}}{\mathrm{d}s} (\mathfrak{n} \frac{\mathrm{d}}{\mathrm{d}s} \mathbf{r}(s)) = \mathbf{\nabla} \mathfrak{n}$
- Approximation small $\alpha \rightarrow \mathcal{R}$ straight : $\mathbf{r} \cdot \mathbf{p}_{\theta} = \tau$ error < 10% $\alpha(\tau, \theta) = \sin(\alpha)$



$$\alpha(\tau,\theta) = \frac{1}{\mathfrak{n}_{\mathrm{r}}} \int_{\mathbb{R}^2} \left(\boldsymbol{\nabla} \mathfrak{n}(\mathbf{r}) \cdot \mathbf{p}_{\theta} \right) \, \delta(\tau - \mathbf{r} \cdot \mathbf{p}_{\theta}) \, \mathrm{d}^2 \mathbf{r}$$

 $\frac{\text{Deflectometric Central Slice Theorem:}}{y(\omega, \theta) := \int_{\mathbb{R}} \alpha(\tau, \theta) e^{-2\pi i \tau \omega} d\tau = \frac{2\pi i \omega}{\mathfrak{n}_{r}} \,\widehat{\mathfrak{n}}(\omega \, \mathbf{p}_{\theta})}$ $\widehat{\mathfrak{n}}(\omega \, \mathbf{p}_{\theta}) : 2\text{-D Fourier transform of }\widehat{\mathfrak{n}} \text{ in Polar grid}$

Discrete Forward Model

- $\mathbf{n} \in \mathbb{R}^N$; Cartesian grid of $N = N_0^2$ pixels; sampling: δr
- $\mathbf{y} \in \mathbb{R}^{M}$; Polar grid of $M = N_{\tau}N_{\theta}$ pixels; sampling: $\delta \tau$, $\delta \theta$

• **D**:
$$\frac{2\pi i (\delta r)^2}{\mathfrak{n}_r}$$
 diag $(\omega_{(1)}, \cdots, \omega_{(M)}) \in \mathbb{C}^{M \times M}$

- $\mathbf{F} \in \mathbb{C}^{M \times N}$: Non-equispaced Fourier Transform (NFFT) [4]
- η ∈ C^M : numerical computations, model discretization, model discrepancy, observation noise

[4] J. Keiner et al. (2009)

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ODT vs. AT

$$\mathsf{y} = \mathsf{DFn} + \eta$$

- Main difference: Operator **D**
- ullet Without noise $\eta
 ightarrow$ classical tomographic model

$$\tilde{\mathbf{y}} = \mathbf{D}^{-1}\mathbf{y} = \mathbf{F}\mathbf{n}$$

- For $\eta
 eq 0
 ightarrow$ Not a classical tomographic model
 - η : AWGN $ightarrow {\sf D}^{-1}\eta$ not homoscedastic

ODT vs. AT

UCL Université catholique de Louvain Observation: 1-D FT of sinograms along the τ direction



Standard Reconstruction Methods

 $\mathsf{y} = \mathbf{\Phi} \mathfrak{n} + \eta = \mathsf{DF} \mathfrak{n} + \eta$

1. Filtered Back Projection

- Analytical method
- Solution $\tilde{\mathfrak{n}}_{\mathsf{FBP}}$:

Problems:

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- Filtering the tomographic projections
 - AT: ramp filter; ODT: Hilbert filter
- Backprojecting in the spatial domain by angular integration

2. Minimum Energy Reconstruction

$$\tilde{\mathfrak{n}}_{\mathsf{ME}} = \mathbf{\Phi}^{\dagger} \mathbf{y} = \mathbf{\Phi}^{*} (\mathbf{\Phi} \mathbf{\Phi}^{*})^{-1} \mathbf{y} \equiv \tilde{\mathfrak{n}}_{\mathsf{ME}} = \arg\min_{\mathbf{u} \in \mathbb{R}^{N}} \|\mathbf{u}\|_{2} \, \text{s.t.} \, \mathbf{y} = \mathbf{\Phi} \mathbf{u}$$

Noise

- Compressiveness $\Rightarrow M(N_{\theta}) < N$
 - \Rightarrow ill-posed problem

Solution: Regularization

Sparsity prior

Heterogeneous transparent materials with slowly varying refractive index separated by sharp interfaces





Intraocular lenses

Optical fibers

TV and BV promote the perfect "cartoon shape" model



"Sparse" gradient Small Total Variation norm

 $\|\mathbf{n}\|_{\mathsf{TV}} := \|\mathbf{\nabla}\mathbf{n}\|_{2,1}$



Other priors

• Positive RIM

UCL Université catholique $\Rightarrow \mathfrak{n} \succeq 0 \qquad (\mathrm{no} \ \mathrm{metamaterial} \ \mathrm{here} \ ;-)$

• The object is completely contained in the image. Pixels in the border are set to zero in order to guarantee uniqueness of the solution.

 $\Rightarrow \mathbf{n}|_{\delta\Omega} = 0 \quad \text{(up to an intensity shift)}$

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$TV-\ell_2$ reconstruction and Noise

$$\mathsf{y} = \mathbf{\Phi} \mathfrak{n} + \eta = \mathsf{DF} \mathfrak{n} + \eta$$

TV- ℓ_2 Reconstruction

$$\tilde{\mathbf{n}}_{\mathrm{TV}-\ell_2} = \underset{\mathbf{u}\in\mathbb{R}^N}{\arg\min\|\mathbf{u}\|_{\mathrm{TV}}} \text{ s.t. } \|\mathbf{y}-\mathbf{\Phi}\mathbf{u}\|_2 \leq \varepsilon, \ \mathbf{u}\succeq \mathbf{0}, \ \mathbf{u}_{\partial\Omega}=\mathbf{0}$$

Noise

• Observation noise $\rightarrow \sigma^2_{\rm obs}$

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- Modeling error ightarrow ray tracing with Snell law pprox 10%
- Interpolation noise \rightarrow NFFT error (very small)
- + Reconstruction using CP algorithm [5] expanded in a product space

[5] A. Chambolle and T. Pock. Journal of Mathematical Imaging and Vision. (2011)

Synthetic Results

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Compressiveness and noise robustness



Synthetic Results

- No measurement noise (MSNR $= \infty$)
- $N_{\theta}/360 = 25\%$

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Synthetic Results

- No measurement noise (MSNR $= \infty$)
- $N_{\theta}/360 = 5\%$



x 10⁻³

10

8

6

4

2

0

-2



- Bundle of 10 fibers immersed in an optical fluid
- MSNR pprox 10dB
- $N_{\theta} = 60 \Rightarrow N_{\theta}/360 = 17\%$





- Bundle of 10 fibers immersed in an optical fluid
- MSNR \approx 10dB

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UCL Université catholique de Louvain • $N_{\theta} = 60 \Rightarrow N_{\theta}/360 = 17\%$







- Bundle of 10 fibers immersed in an optical fluid
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- Bundle of 10 fibers immersed in an optical fluid
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Summary and further work (1/2)

- Optical Deflectometry Tomography benefit of sparse regularization!
- ▶ Robust "Compressiveness" is allowed but ...
 - ► NFFT mandatory!
 - careful noise estimation is needed (not explained here)
 - non-linearities remain (handled as noise up to now)



Summary and further work (2/2)

- Other applications?
 - Phase-contrast X-ray imaging (deflection \rightarrow phase change)



[T. Pfeiffer et al. Nature Physics, 2006]



Summary and further work (2/2)

- Other applications?
 - Phase-contrast X-ray imaging (deflection \rightarrow phase change)

• Gravitational weak lensing?





[T. Pfeiffer et al. Nature Physics, 2006]

[A. Amara, A. Réfrégier, "Optimal surveys for weak-lensing tomography", MNRAS, 381(3), 1018-1026.]

Thank you!



Further readings

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